

Measurement problems encountered in TAT clinical practice

Medical Physics

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Measurement problems encountered in TAT clinical practice

Medical Physics

Measuring the patient-specific and daughter-specific pharmacokinetics



Patient-specific dosimetry

Pharmacokinetics

Imaging

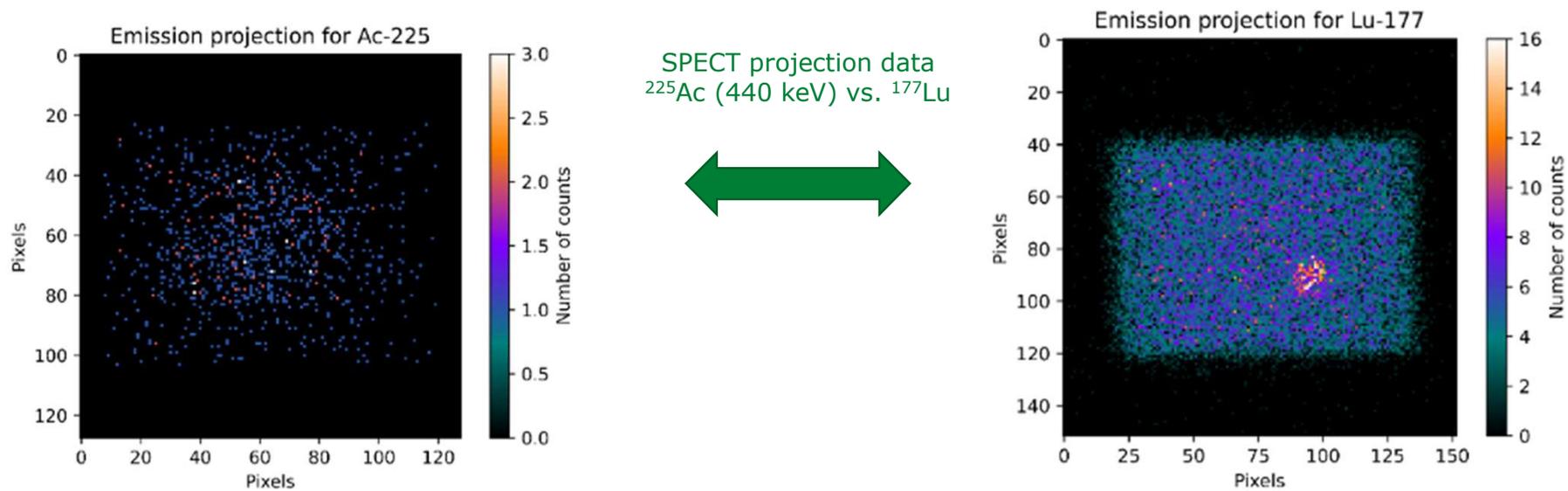
	[¹⁷⁷ Lu]Lu-PSMA-I&T	[²²⁵ Ac]Ac-PSMA-I&T	²²⁵ Ac vs. ¹⁷⁷ Lu signal SPECT
Therapeutic activity	7.4 GBq	8 MBq	≈ 1/1000
Photon yield	208 keV: 10 % (113 keV: 6 %)	218 keV: 11 % 440 keV: 26 %	≈ 1/1000* ≈ 1/500*
			*compared to ¹⁷⁷ Lu 208 keV

- Direct patient-specific imaging is doable but challenging in clinical routine
- Example for [²²⁵Ac]Ac-PSMA:
 - Photon yield comparable to e.g. ¹⁷⁷Lu but
 - Low therapeutic activities limit signal strength for Gamma camera imaging
 - 440 keV challenging for a conventional gamma camera system

Pharmacokinetics

Imaging

- Comparison of SPECT projection data for NEMA phantom filled with clinically realistic activities



Pharmacokinetics

Imaging

- Comparison of SPECT projection data for combined $^{177}\text{Lu}/^{225}\text{Ac}$ -PSMA-I&T treatment (1000 MBq vs. 8 MBq)

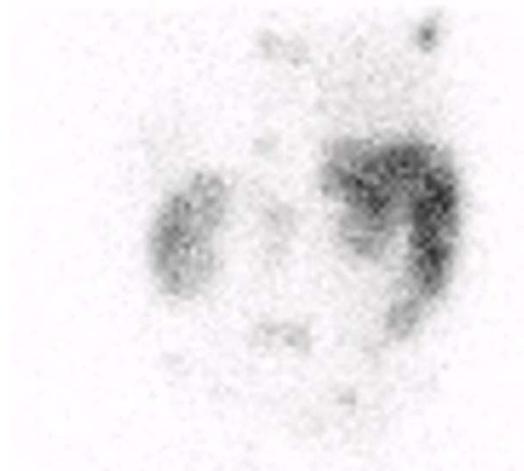
^{225}Ac 440 keV (width 20 %)
3.5 minutes p. projection



SPECT projection data
 ^{225}Ac vs. ^{177}Lu



^{177}Lu 208 keV (width 15 %)
3.5 minutes p. projection



Pharmacokinetics

Current clinical qSPECT/CT protocol @ LMU for ^{225}Ac

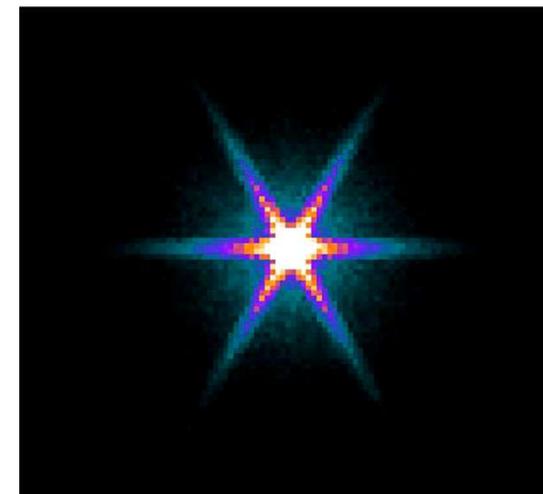
- Current clinical qSPECT/CT protocol @ LMU for [^{225}Ac]Ac-PSMA-I&T and ^{225}Ac -PRRT
 - High-energy collimator, 3/8" crystal (Siemens Intevo T16 and Symbia T2 SPECT/CT)
 - 32 projections for 360°
 - 128 x 128 pixels ($\sim 4.8 \times 4.8 \text{ mm}^2$)
 - 210 sec per projection → ~ 1 hour total acquisition time!
 - 440 keV +/- 10 % (+ lower scatter), 218 keV +/- 10 % (+ lower/upper scatter), 78 keV +/- 25 %
- **Current clinical restrictions**
 - Field-of-view is limited to one bed position only
 - Comfortable patient positioning is crucial
 - Imaging not available for all patients/all therapy cycles
 - Late imaging challenging

Pharmacokinetics

Current clinical qSPECT/CT protocol @ LMU for ^{225}Ac

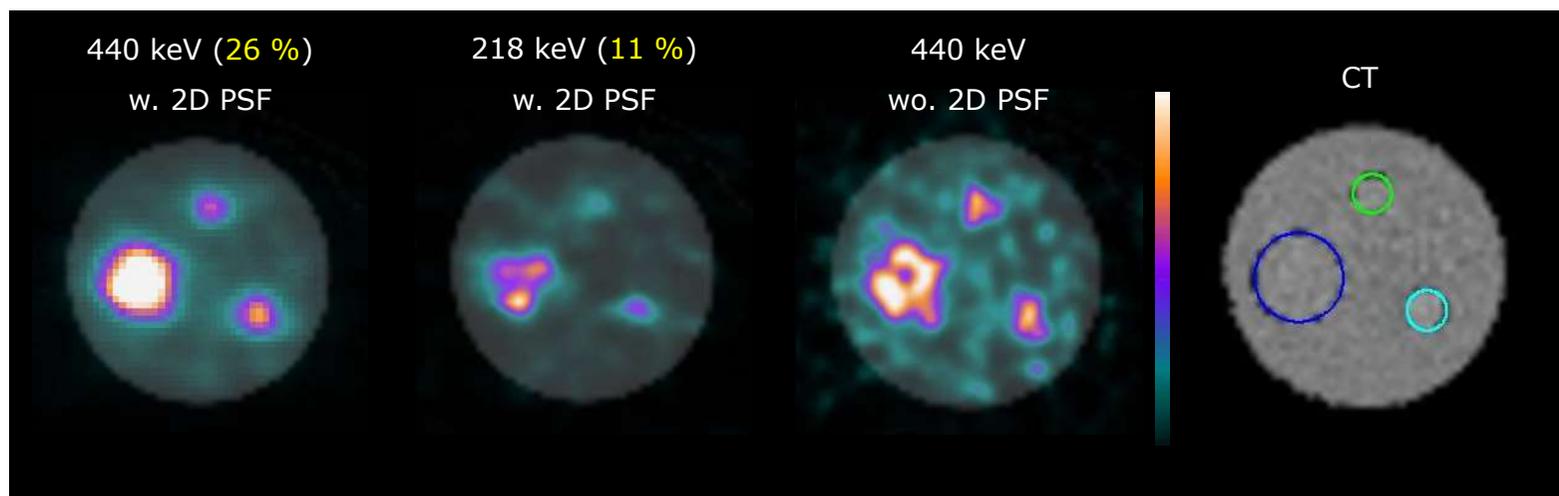
- Quantitative reconstruction
 - In-house MAP-EM (plus additional post-filtering)
 - 2D presimulated (SIMIND) point-spread-function set for resolution modelling (steps of 0.4 cm up to 60 cm distance; 10^{10} primaries for 128x128 pixel)
 - Transmission-dependent scatter correction

2D detector point-spread function
@ 440 keV



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2D resolution modelling for ^{225}Ac qSPECT



- **High count measurement:** 30-fold higher activity concentration than expected in clinical routine (200 Bq/ml 72 h p.i. OAR)
- → total activity of approx. 2.8 MBq, ratio approx. 6:1

Pharmacokinetics

Measuring scatter for ^{225}Ac

Ann Nucl Med (2008) 22:549–556
DOI 10.1007/s12149-008-0170-z

ORIGINAL ARTICLE

Three-dimensional SPECT reconstruction with transmission-dependent scatter correction

Antti Sohlberg · Hiroshi Watabe · Hidehiro Iida

- Energy-window based scatter correction is likely to add **additional noise** (more severe for 218 keV)
- → **Transmission-dependent scatter correction** based on current image estimate (Sohlberg et al., Ann. Nucl. Med. 2008)

^{225}Ac 440 keV (width 20 %)
3.5 minutes p. projection



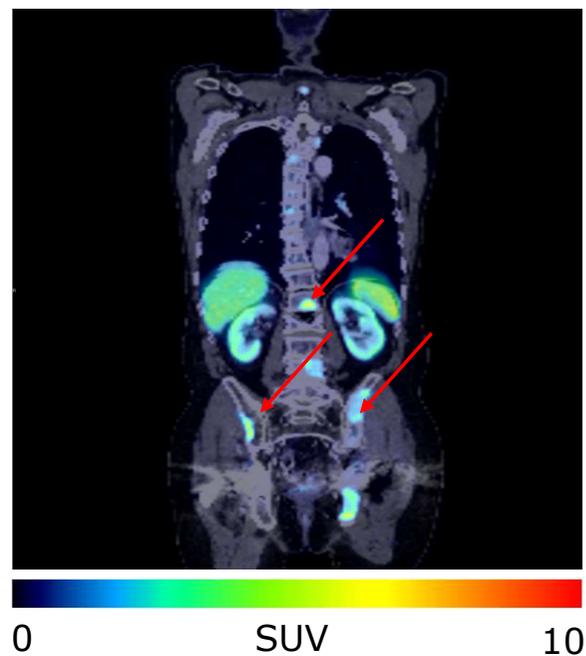
^{225}Ac 440 keV **lower scatter** (width 20 %)
3.5 minutes p. projection



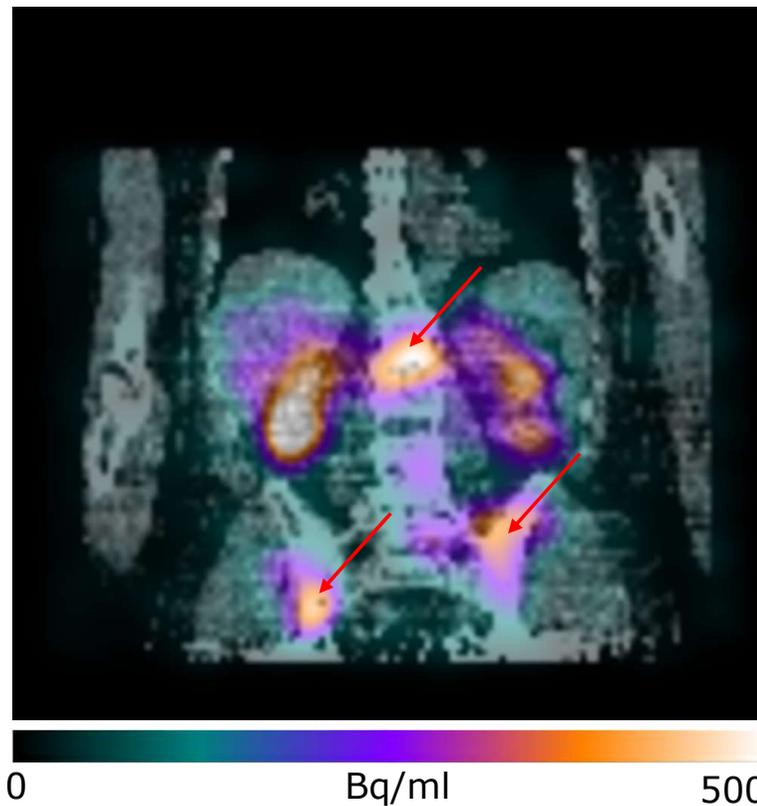
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Patient example [²²⁵Ac]Ac-PSMA-I&T SPECT/CT @ 24 h p.i. (8 MBq)

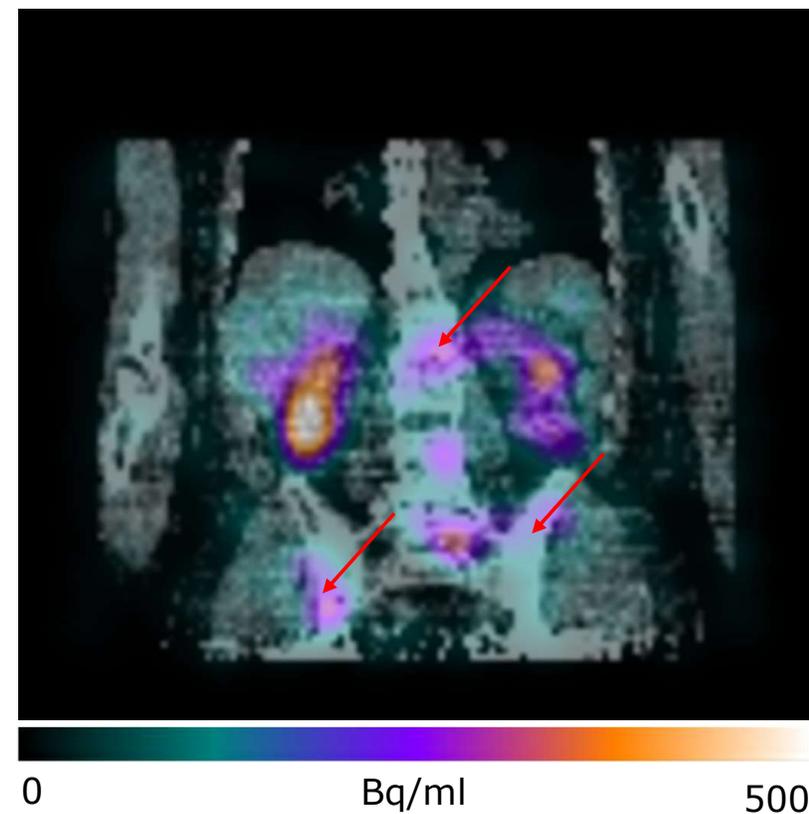
Pre-therapeutic PET-CT



218 keV TDSC

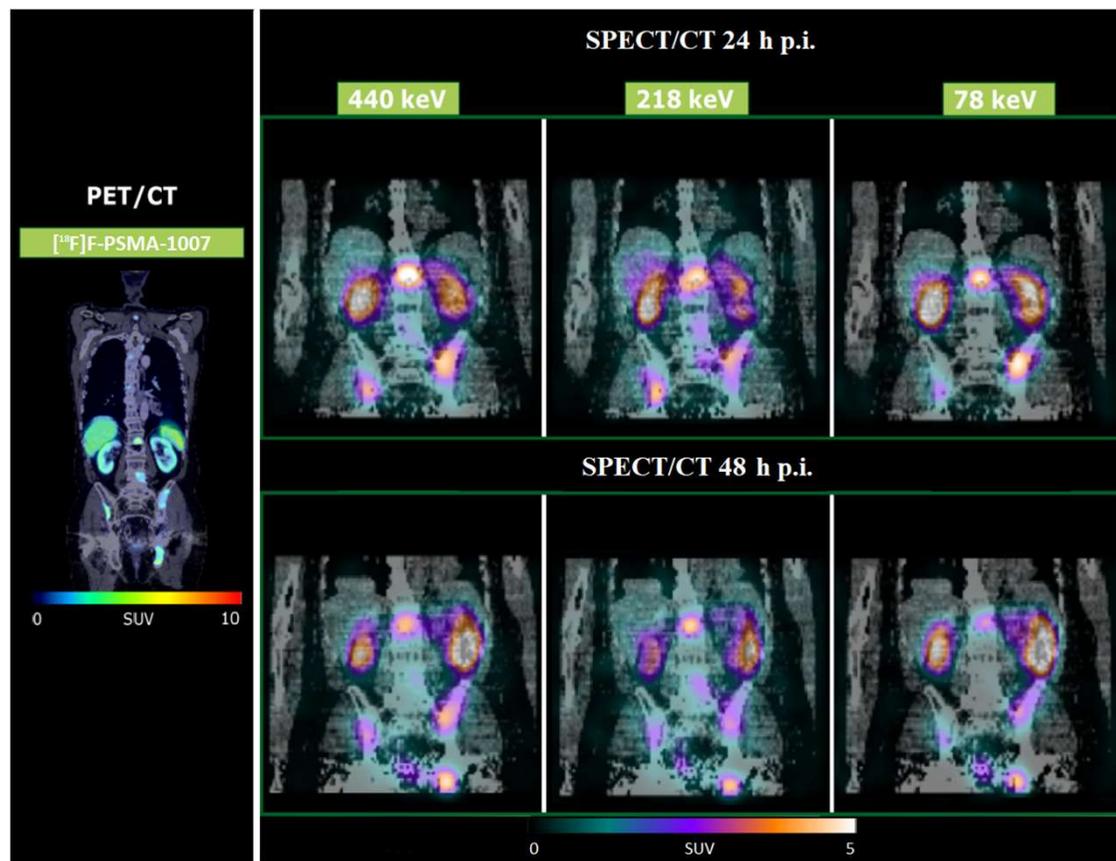


218 keV TEW



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Patient example [^{225}Ac]Ac-PSMA-I&T SPECT/CT (8 MBq)



Liubchenko et al., under review, EJNMMI

Pharmacokinetics

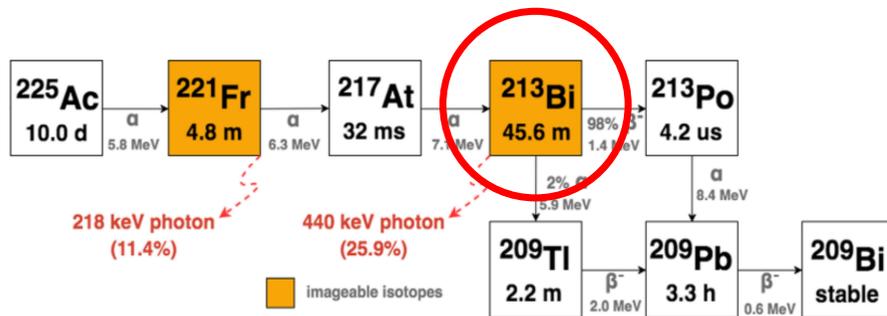
- Direct patient-specific imaging is doable but challenging in clinical routine)
- Surrogate imaging using theranostic pairs (e.g. [^{177}Lu]Lu-PSMA for [^{225}Ac]Ac-PSMA (Kratochwil et al. 2017), [^{64}Cu]Cu-FAPI-04/[^{225}Ac]Ac-FAPI-04 (Watabe et al. 2020)...)
 - → knowledge about target expression and target vector pharmacokinetics
 - → limited knowledge about daughter-specific pharmacokinetics
- In-vivo sampling (e.g. blood, urine)

Or combinations of both
for more efficient and
reliable protocols

Pharmacokinetics

Daughters

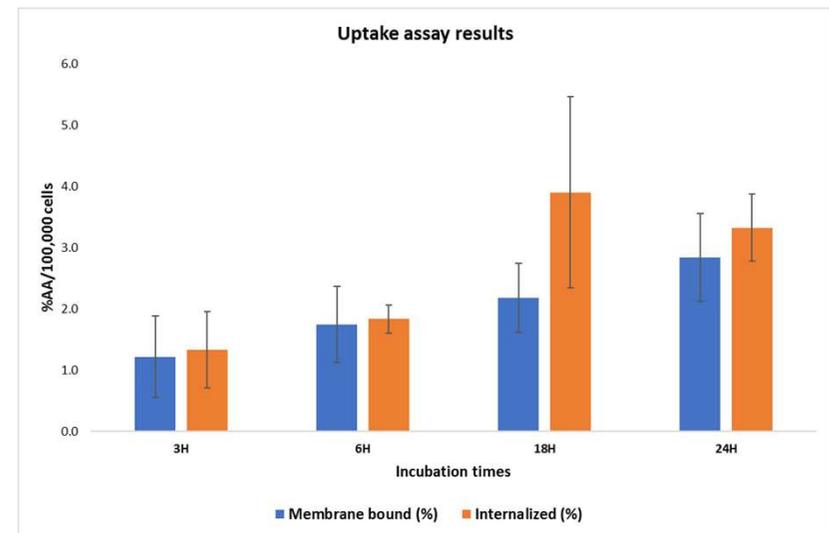
- ^{223}Ra , ^{225}Ac ,... → long decay chains with alpha-emitting, long-lived daughters
- Ignoring free daughters can change tumor-to-OAR dosimetry
- Cell internalization is an important parameter



Robertson et al., PMB, 62 (11), 2017

Free ^{213}Bi accumulates in kidneys!

$[^{177}\text{Lu}]\text{Lu-PSMA-I\&T}$ in LNCaP

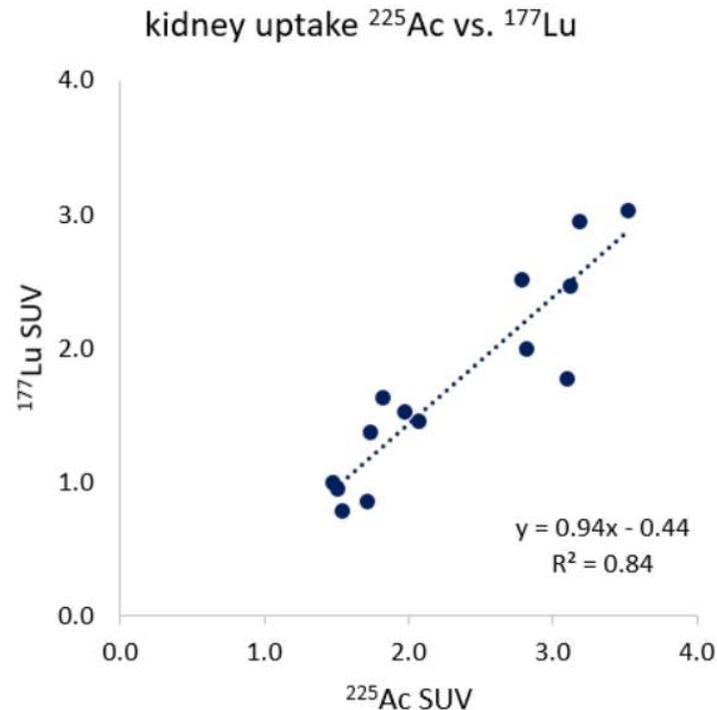
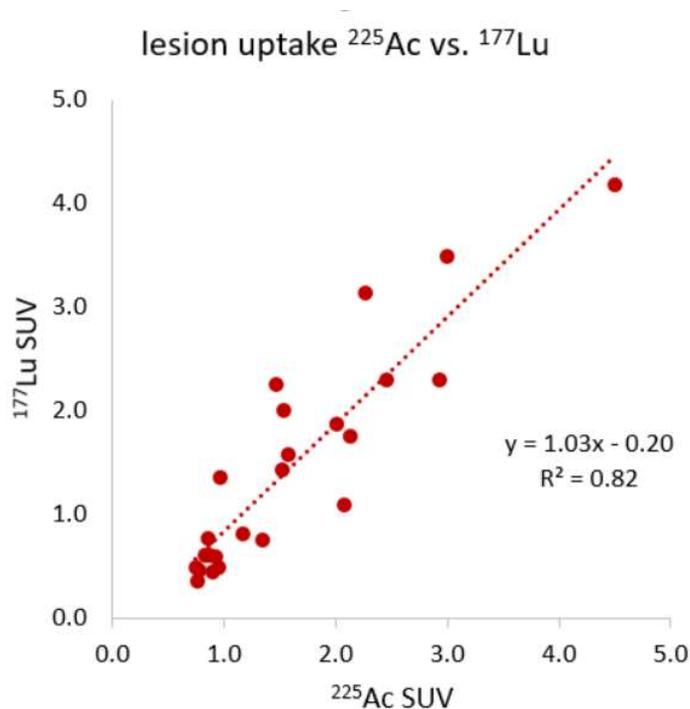


Hawarihewa et al., upcoming German congress (Nuklearmedizin 2024)

Pharmacokinetics

Multi-isotope SPECT for combined $^{177}\text{Lu}/^{225}\text{Ac}$ -PSMA therapy

- 7 patients w. SPECT imaging 24 h p. i. 208 keV (^{177}Lu) and 440 keV (^{225}Ac)
- 14 kidneys and 24 lesions (bone and lymph node metastases)



	^{213}Bi SUV _{mean} (st. dev.)	^{177}Lu SUV _{mean} (st. dev.)
Kidneys	2.3 (0.7)	1.7 (0.8)
lesions	1.6 (0.9)	1.5 (1.1)

- Strong & significant correlation for both lesions and kidneys ($r > 0.9$, $p < 0.01$)
- Higher kidney uptake for 440 keV → free ^{213}Bi ?

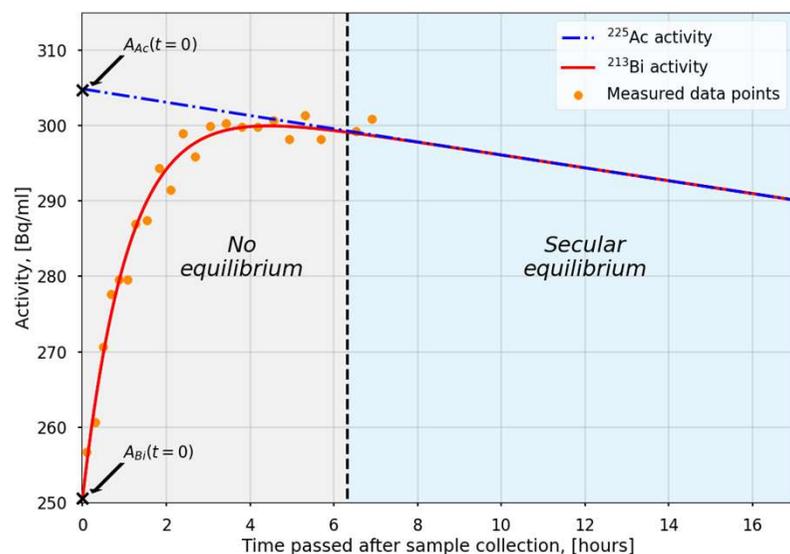
no recovery correction applied & images filtered to match SNR

Delker et al., EJNMMI 2023

Pharmacokinetics

Daughters

- Continuous urine sampling (sample collection along with each SPECT acquisition)



Urine & kidney pharmacokinetics [^{225}Ac]Ac-PSMA-I&T (5 patients)

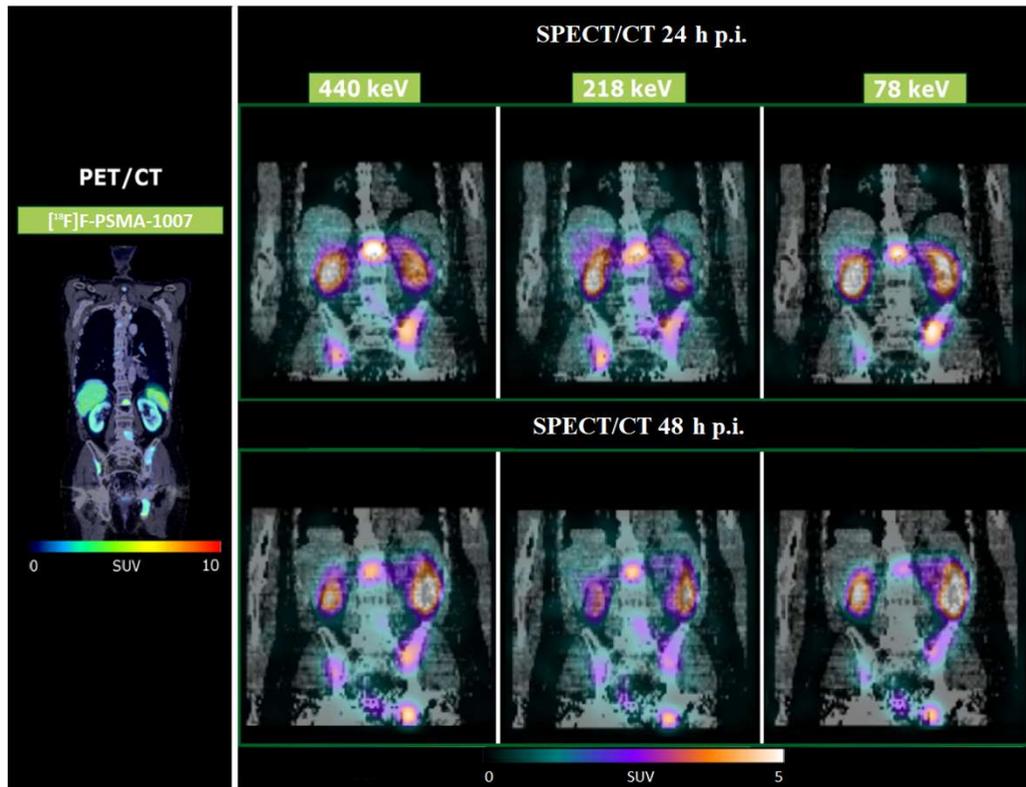
	% increase from 24 to 48 h p.i.	24 h	48 h
^{213}Bi -to- ^{225}Ac ratio urine	10 ± 9	0.98 ± 0.15	1.08 ± 0.09
^{213}Bi -to- ^{221}Fr renal ratio	9 ± 8	1.08 ± 0.10	1.18 ± 0.10
SUV_{mean}			

Liubchenko et al., under review, EJNMMI

- Patient-specific blood sampling is challenging for 24 h p.i. and later

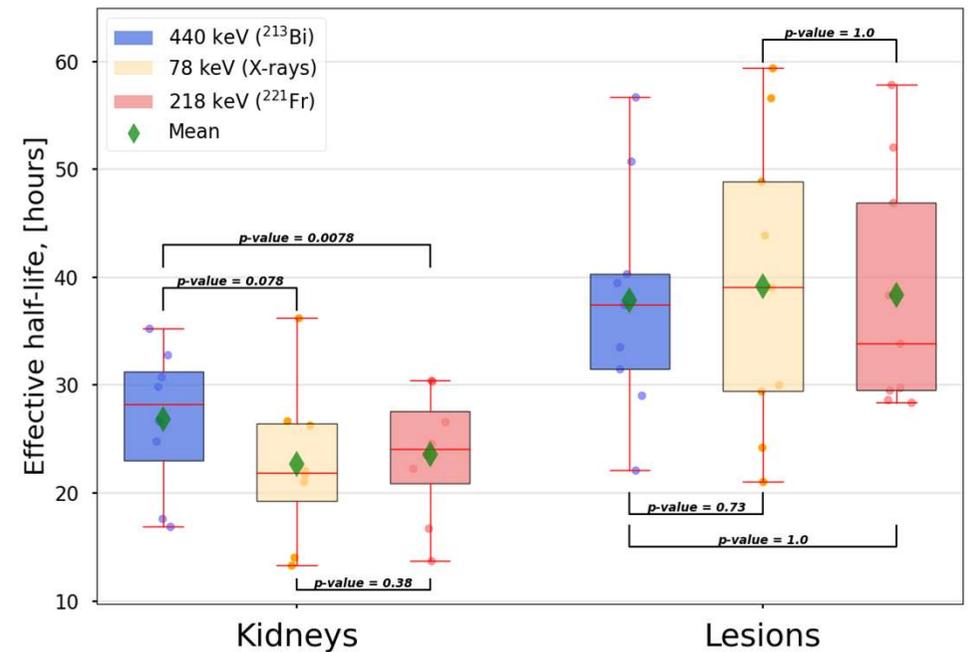
Pharmacokinetics

Daughters



Liubchenko et al., under review, EJNMMI

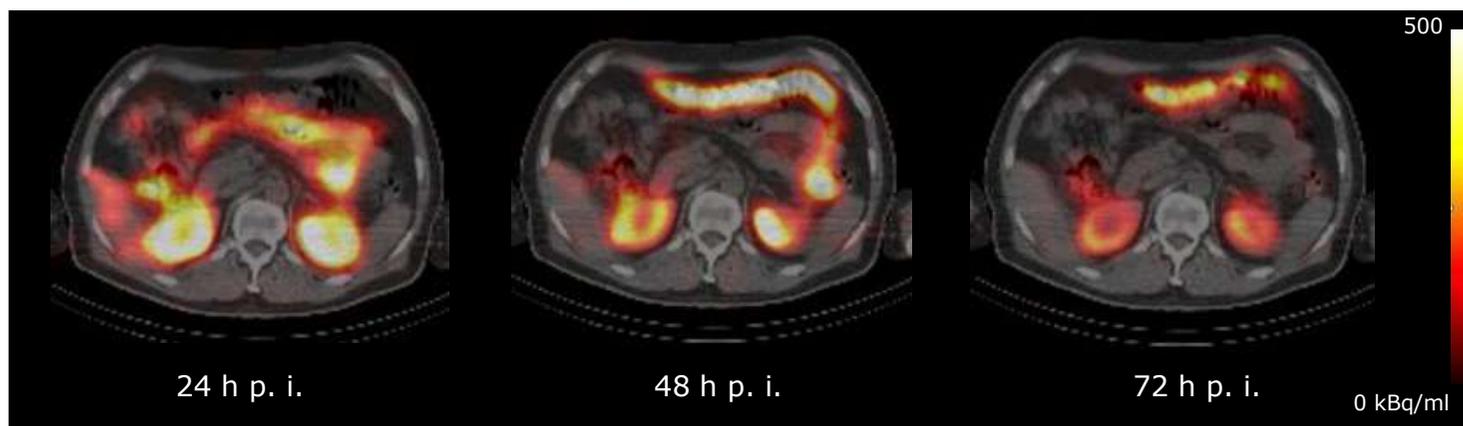
Five patients with [²²⁵Ac]Ac-PSMA-I&T (8 MBq) qSPECT @ 24 and 48 h p.i.



- Renal effective half-lives and SUV show significant correlation for ²¹³Bi and ²²¹Fr
- Significantly higher renal effective half-lives for ²¹³Bi

From imaging to patient-specific dosimetry...?

- For alpha emitters, dosimetry requires knowledge of the cellular and subcellular pharmacokinetics
- Problem: clinical imaging devices are limited to a resolution of mm to cm



SPECT-based kidney dosimetry for $[^{177}\text{Lu}]\text{Lu-PSMA}$ therapy (6 GBq)

$$RBE - \text{weighted dose [Sv]} = \text{Absorbed dose [Gy]} \times RBE \quad ?$$

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Conclusion

- Measurement of the patient-specific and daughter-specific pharmacokinetics is doable, but
 - Long acquisition times → limited field-of-view, no. of time points/patients currently restricted
 - Late imaging particularly difficult for TAT with low activities
 - Reconstruction algorithms need to be adapted for low-count regime and high-energy gammas
 - Surrogate imaging needs careful interpretation for complex decay chains with long-lived daughters
- Clinical imaging limited to a resolution of a few mm up to cm → **How to connect macro- and microdosimetry?**
- Which RBE (tissue-specific, endpoint-specific,...)?

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